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Interfacing microfluidic chip-based chromatography with flame atomic absorption spectrometry for the determination of chromium(VI)

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SPECTIVE TO THE determination of chromium (VI)

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1 N F 14 This work demonstrates the first study on interfacing of microfluidic chip-based chromatography to flame atomic absorption spectrometry (FAAS) for a simple and fast separation or preconcentration and subsequent determi-16 nation of species. The developed low-cost polydimethylsiloxane microchip includes 12 microcolumns of 17 conventional C18 (5 μm) chromatographic particles, making the parallel chromatographic separation/ preconcentration and the direct introduction of the effluent into the spectrometer possible. In order to test 18 this hyphenated microchip–FAAS system, the Cr(VI) was selected to be determined. The adsorbed Cr(VI) was 19 eluted with methanol, and the 30 μL effluents were collected into plastic vessels inserted into the ends of the 20 microcolumns. Then, the effluents were analyzed by FAA spectrometer using micro-injection of the effluents 21 as discrete samples. The separation/preconcentration and FAAS determination of 12 samples needed less than 22 5 min due to the multiplex feature of the proposed system. The overall capacity of the microcolumn (C18, 23 5 μm beads, 20 mm \times 1 mm \times 0.1 mm) was calculated to be 0.45 μg/mm for Cr(VI). Loading only 80 μL samples 24 onto the microchip and nebulizing the methanolic effluent of 30 μL into the FAA spectrometer, 0.0031 μg/mL 25 limit of detection was obtained. 26

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32 1. Introduction

 Microfluidic devices have emerged as novel analytical tools in many areas of biomedical or environmental monitoring. These cheap devices have low power requirements and low sample/reagent consumption and provide the possibilities of fast and possible parallel analysis. For the microfluidic devices, only detectors which have (i) reduced diffu- sion length between the chip and the detection cell and (ii) the ability to require only a few microliters or submicroliter of sample can be ap- plied. The applicability of many different electrochemical [1], optical 41 and mass spectrometric [2] detection methods has been demonstrated 42 in the last two decades. Since atomic spectrometers typically need at least a few hundreds of microliters for analysis, relatively small number of works can be found in literature about the element-selective detec- tors hyphenated with microchips. Inductively coupled plasma-mass spectrometry (ICP-MS) has been coupled to chip-capillary electropho- resis for speciation analysis [\[3,4\]](#page-5-0). Recently, chip-based magnetic solid- phase extraction was applied before the determination of selenium spe- cies using high-performance liquid chromatography (HPLC)-ICP-MS [\[5\].](#page-5-0) Besides the ICP-AES or ICP-MS detectors, only one work was found using other type of atomic spectrometric method for interfacing with microchip: Li et al. [\[6\]](#page-5-0) coupled (flameless) atomic fluorescence spec-trometry to microchip, in which electrophoretic separation of mercury

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species was carried out and the effluents were converted to volatile 54 components. However, no combination of microfluidic chip with the 55 traditional and often used flame atomic absorption spectrometer 56 $(FAAS)$ was found.

Despite the high demand for miniaturized liquid chromatographic 58 (LC) techniques, there are only a few chip-based chromatographic sys- 59 tems compared to chip-based capillary electrophoretic devices [\[7\].](#page-5-0) 60 First, Manz et al. [8] described an LC partially integrated onto a silicon 61 chip in which chromatographic C8 particles were retained by frits in 62 the column. Other devices have incorporated a physical barrier [\[9\],](#page-5-0) 63 tapered capillary geometries [10] or fritless bottleneck [\[11,12\]](#page-5-0) to trap 64 stationary-phase particles. Hansen et al. [\[13\]](#page-5-0) reported microfluidic 65 solid-phase chromatography columns formed by multilayer soft lithog- 66 raphy. Recently, our group has demonstrated the preparation of simple 67 and permanent multiple chromatographic columns that are suitable for 68 parallel chromatographic separations without frits [\[14\]](#page-5-0).

Chromium provides a typical example for how the different oxida- 70 tion forms of the same element may show highly different toxicity: in 71 biological systems, Cr(III) is essential while it is a definitely carcinogenic 72 element in the form of $Cr(VI)$ [\[15\].](#page-5-0) Therefore, the accurate individual 73 determination of Cr(VI) is important. For chromium speciation, one of 74 the most effectively used techniques is the on-line combination of HPLC 75 separation with the element-selective detection of atomic spectrometry 76 [16–[18\].](#page-5-0) Following the labour- and time-consuming, yet less accurate ex- 77 traction, ion-exchange and co-precipitation methods [\[19,20\],](#page-5-0) in the last 78 two decades, several papers have been published on the combination of 79

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 chromatography and element-selective detection [\[21,22\]](#page-5-0). The on-line chromatographic separation/preconcentration of Cr(VI) with FAAS detec- tion has been published by Posta et al. [\[18,23\]](#page-5-0). This preconcentration method is based on the ion pairs formed by Cr(VI) with tetrabutylammonium (TBA) salts, as these complexes can be sorbed on C18. After the sorption, the Cr(VI) is eluted with methanol and intro-duced into the spectrometer.

 Our work aims at developing a low-cost, microchip-based multiple chromatographic technique that can be coupled with a flame atomic absorption spectrometer. In order to test this system, the toxic Cr(VI) was chosen to be separated/preconcentrated on the microchip prior to the FAAS determination.

92 2. Experimental

93 2.1. Apparatus and reagents

 Determination of chromium was carried out with a 240FS atomic ab- sorption spectrometer (Agilent Technologies, Santa Clara, CA, USA) equipped with flame atomization (a mixture of air (13.5 L/min) and acet- ylene (2.9 L/min)). The chromium hollow cathode lamp (Cathodeon) op- erated at a current of 10 mA. Chromium was determined on the wavelength of 357.9 nm with a spectral bandwidth of 0.2 nm. Deuterium correction of background was used, and the signal was measured in an integration mode for 30 s. Signal peaks were recorded by the software of the spectrometer (SpectrAA 5.2 Pro, Agilent), and figures showing 103 the signals demonstrated in this work were cut from the report automat-ically generated by the software.

105 Solution of Cr(VI) was prepared by the dilution of a 1000 mg/L potassium dichromate stock solution produced by Fluka. A detailed description of the chromatographic separation/preconcentration meth- od of Cr(VI) was provided in an earlier publication [18]. The ion pair complex of Cr(VI) with TBA salts (Sigma) was retained quantitatively on a microchip-based C18 microcolumn (Varian 100-C18 5 μm) in an 111 acetic acid medium at pH 3 in the presence of $5 \cdot 10^{-2}$ mol/L TBA. After loading the sample onto the microcolumn, the adsorbed Cr(VI) was eluted with methanol (VWR) and transferred to the FAA spectrometer.

115 2.2. Preparation of multiple chromatographic packings in a microchip

 Microfluidic chips made from polydimethylsiloxane (PDMS) were prepared by using a mold created by soft photolithography mainly according to the procedure described by Whitesides [24]. The channel pattern was printed as a high-resolution (4000 dpi) photomask. In order to get a thickness of around 100 μm (that is, much thicker than usual in microfluidics), the negative type photoresist (SU-8 2025, Microchem, Newton, MA) was spin-coated onto a 3″ silicon wafer only with 500 rpm for 30 s. The PDMS chip was fabricated by a cast molding of a 10:1 mixture of PDMS oligomer and cross-linking agent (Sylgard 184, Dow Corning, Midland, MI). The PDMS chip was sealed onto a glass slide of 1.2 mm thickness after oxygen plasma treatment 127 (PDC-32G, Harrick, Ithaca, NY).

 The microchip includes 12 parallel channels (width: 1 mm, height: 100 μm), which merge into a single port E (elution) of a 0.3 mm diam- eter. At the other end of each channel, similar ports S (sample) are created by punching the PDMS, and a compressed small cotton wool (<1 μ g) serving as a frit for retaining the chromatographic particles is pressed down to the bottom of the port [\(Fig. 1a](#page-2-0)) using a metal rod.

 For the preparation of chromatographic packing, similar process was 135 applied to the one used in our earlier works [\[14\]](#page-5-0). The 12 channels of the microchip were packed simultaneously from port E, pumping a single plug of C18 suspension splitted toward the other ends of the parallel channels. Briefly, a suspension (~100 μL) of freshly ultrasonicated, 139 methanolic C18 particles of 5 μm was manipulated through a small-bore tubing (0.25 mm ID) using a peristaltic pump. The tubing was connected to the port E ([Fig. 1a](#page-2-0),b), and the particles were washed 141 with methanol $(-10 \mu L/min)$ toward the frit at the end of the channels 142 (ports S). The obtained packing (microcolumn) was rinsed with metha- 143 nol with intermittent $(4-5 s)$ application of pumping pressure (-2 bars) 144 to improve the compactness of the packing. The packings were condi- 145 tioned with 10 min washing with methanol and 5 min with the mobile 146 phase before the chromatographic separation/preconcentration. A sche- 147 matic depiction of the packing preparation procedure and the picture of 148 the obtained microchip are given in [Fig. 1](#page-2-0)a,b. 149

Samples to be analyzed should be injected to the microcolumns 150 through the S ports using peristaltic $pump(s)$. It is possible to inject 151 even 12 different samples parallelly to separate chromatographic pack- 152 ings (6- or 8-channel peristaltic pumps are quite common in the market). 153 Then, the adsorbed (preconcentrated) Cr(VI) can be eluted from the 154 microcolumn by pumping the eluent from the common port E (elution). 155 In this case, all adsorbed Cr(VI) will be eluted from all microcolumns at 156 the same time, but the elution from a given channel can be prevented 157 by blocking the port S of any microcolumns. A schematic depiction of 158 the sample loading and elution is given in Fig. 1c. 159

The adsorbed amounts of Cr(VI) were eluted into small hydrophobic 160 plastic vessels (5 mm part length of the bottom of a 0.1-mL polypropyl- 161 ene micropipette tip, \sim 40 μL) positioned just at the ends of the chro- 162 matographic microcolumns (Fig. 1d). The plastic vessels could be 163 easily and tightly inserted into the flexible ports S; no leakage outside 164 around the vessel could be observed. Since the inner diameter of the 165 funnel-shape vessel gradually reduced from 3 mm to 0.4 mm, the end 166 of the sampling capillary of the pneumatic nebulizer of the FAA spec- 167 trometer could be simply introduced into the lower part of the vessel. 168 The liquid content of the plastic sampling vessel was instantly sucked 169 out by the PTFE capillary of the nebulizer when it was immersed into 170 the vessel. The length of the capillary was reduced to 10 cm to minimize 171 the dispersion of the liquid sample on the surface of the capillary 172 between the microchip and the nebulizer (Fig. 1e). 173

3. Results and discussion 174 174

3.1. Harmonizing the sample volume needed for FAAS to the sample volume 175 eluted from the chip-based chromatographic packings 176

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angle of the starting due to consume per solution per signator ($\frac{1}{2}$ and the starting of the sta With FAA pneumatic nebulizers, samples are taken up continuously 177 consuming a few milliliters of sample. After a few seconds of aspiration 178 (several hundreds of μL of the sample), a continuous signal can be ob- 179 tained. However, small \langle (200μ L) sample volumes can also be injected. 180 The small volumes of the samples were injected from a funnel or 181 hemisphere-shape cup made from a hydrophobic PTFE plate. Various 182 researches [25,26] have studied this micro-injection technique of 183 discrete samples, proving that the nebulization of a 100 μL sample 184 gives the same sensitivity as the one obtained by conventional nebuliza- 185 tion. Others [27] reported that using even a 60 μL volume of a sample the 186 maximum sensitivity can be achieved with a better precision than 1.5 187 RSD%. The peak height of the analytical signal depends on the injected 188 volume, the wetting of the surface of the sampling vessel and the nebu- 189 lizer capillary by the liquid sample as well as the solution flow rate of 190 the nebulizer. 191

The small volumes of the samples were injected to small hydropho- 192 bic plastic vessels (cup) by a micropipette (Biohit). The end of the PTFE 193 capillary of the nebulizer was immersed into the bottom of the 194 microsampling cup, then the whole volume of the liquid was complete- 195 ly and immediately sucked into the nebulizer providing a transient sig- 196 nal. The signals rose sharply, and then fast declining with some tailing 197 could be observed due to the dilution of the aerosol at the signal end. 198 In [Fig. 2](#page-2-0), the effect of the injected sample volume (10–100 μL) on the 199 absorption signal for 5 μ g/mL Cr(VI) using micro-injection of the 200 discrete samples is shown. The spike-like signals largely increase with 201 the injected volume up to 30–35 μL and then the increase gets smaller, 202 while the signal intensities for the sample volumes above 100 μL remain 203

Fig. 1. (a,) Schematic (not scale-true, side-view) and the picture (top-view) (b,) of the PDMS microchip including C18 chromatographic packings (20 mm \times 1 mm \times 0.1 mm, 5-µm beads, port S is for sample IN or elution OUT; port E is for waste or elution pumping). (c,) The samples are parallelly injected to the microcolumns through the S ports (loading), and then the adsorbed Cr(VI) can be eluted by pumping the eluent from the common port E (elution). (d,) Picture of the elution of Cr(VI) preconcentrated on the chromatographic packing into a plastic vessel for the subsequent direct nebulization into the FAA spectrometer. (e,) Arrangement of the microchip coupled to the FAA spectrometer.

204 constant and equal to that obtained by a larger sample volume or con-205 tinuous nebulization. The reason for the surprisingly good sensitivity 206 for the only 30 μL sample volume should be found in the construction

Fig. 2. The effect of injected sample volume (10–100 μL) on the absorption signal for 5 μg/mL Cr(VI) using micro-injection of the discrete samples.

of the nebulizer of the used FAA spectrometer (240FS, Agilent). Thus, 207 the mass sensitivity obtained for 30 μL was improved by a factor of 11 208 compared to the (continuous) sucking of 0.5 mL sample volume. 209

In Fig. 3a, the signals obtained for standard solutions of 0.5–50 μg/mL 210 Cr are shown. The applied sample volume was 30 μL using micro- 211 injection of the discrete samples. From these data, a 0.0089 μg/mL limit 212 of detection (LOD) and a linear detection range of 0.2–50 μg/mL could 213 be concluded. [Fig. 3](#page-3-0)b shows the signals of a number of 30 μL samples con- 214 taining 4 μg/mL Cr as an example of the reproducibility and the time con- 215 sumption of the measurements (approximately 20 samples/min). The 216 relative standard deviations ($N = 12$) amounted to 2.9% and 3.8% in sig- 217 nal height and signal area, respectively. Of course, better RSD% values 218 could be obtained for 0.5 mL sample volumes considered as continuous 219 sampling (0.9% and 1.1%). These analytical performance data prove that 220 the sensitivity obtained only from 30 μ L sample volume are only 30% 221 worse than using continuous sample introduction, and the precision 222 values are also acceptable. However, by reducing the sample volume 223 below 30 μL, the LOD and precision data become dramatically worse. 224

Although the minimal uptake demand for sensitive FAAS detection is 225 around 30 μL, this sample volume is still enormously large for typical 226

Fig. 3. Signals obtained for standard solutions of 0.5–50 μg/mL Cr (a,) and the signals of repeated determinations of samples containing 4 μg/mL Cr (b,) using micro-injection of the discrete samples (in each case the sample volumes were 30 μL).

 microfluidic applications. In our earlier [11,12] and others' [13] chip- based chromatographic works, even less than 0.1 μL volume of sample 229 was eluted from the microcolumns. In order to increase the effluent volume, the dimensions of microcolumns were maximized. The soft lithographic procedure [24] used for the microchip preparation enables a 0.1 mm maximal height of the microchannel (the SU-8 2025

photoresist was spincoated with a low speed for short time). The 233 width of a microcolumn was increased to 1 mm (in other chip-based 234 chromatographic work, the widths are 0.1 mm [11–[13\]\)](#page-5-0). The length 235 of the microcolumns was limited by the width of the glass slide. 236 After these considerations, the dimension of the microcolumns was 237 20 mm \times 1 mm \times 0.1 mm ([Fig. 1](#page-2-0)b), which was useful to produce efflu- 238 ent (after separation or preconcentration of components) in a range of 239 10–30 μ L. These chip-based chromatographic columns already can 240 serve enough volume of sample for the micro-injection FAAS. 241

3.2. Separation/preconcentration and determination of Cr(VI) 242

The on-line HPLC separation and FAAS detection of Cr(III) and Cr(VI) 243 have been proposed by Posta et al. [18] using a reverse phase C18 244 column (5 μm particle size, 125 mm length, 4.6 mm i.d.) and using 245 TBA salt as ion-pair forming agent. For the separation, 100 μL sample 246 was needed, and more than $50\times$ enrichment factor was achieved 247 using up a sample volume of 5 mL. The applicability of the separation 248 and preconcentration of Cr(VI) in complex sample matrix (seawater) 249 was shown as well [28]. In our work, we used their optimized condi- 250 tions. The carrier solution was an aqueous solution containing 0.1 mM 251 NH₄ acetate at pH 3. After loading the sample to the microcolumn, the 252 Cr(III) and other ionic components of the sample were passing through 253 the microcolumn, while the Cr(VI) was retained. With the miniaturiza- 254 tion of the separation unit, much less sample volume, 10–30 μL and 255 100–300 μL, was necessary for the separation and preconcentration, 256 respectively. 257

In order to visualize the separation/preconcentration process of the 258 Cr(VI) on the C18 microcolumns embedded in the transparent PDMS 259 chip, a mixture of high concentration of Cr(VI) and Cr(III) standard solu- 260 tions of 10 μL volumes is pumped simultaneously to the parallel 261 columns to retain the Cr(VI) (Fig. 4a). Because the chromate has a rela- 262 tively intensive yellow color, by taking a picture of the microchip, a 263 densitogram of each microcolumn can be created by means of a densi- 264 tometric software (e.g. CP Atlas 2.0, freeware thin layer chromatogram 265 evaluation software) [28]. The densitograms, that is the plots of intensi- 266 ty (RGB values) of colors per pixels of the picture of the microcolumn, 267 are shown in Fig. 4c. The yellow area of the $Cr(VI)$ can be simply 268

Fig. 4. (a,) Picture of the chip-based microcolumns, on which the mixture of 0.05-1 mg/mL Cr(VI) and Cr(III) standard solutions of 10 μL volumes is loaded for 4 min to retain (separate) the Cr(VI). (b,) Signals of the effluents obtained with FAA spectrometer using micro-injection of the effluents as discrete samples of 30 μL. Effluents were collected into a plastic vessel inserted into the ends of the microcolumns. (c,) Densitogram of the adsorbed Cr(VI) (measuring the intensity (RGB) of colors on the microcolumns of (a,)). (d,) The calibration plot of the Cr(VI) standard solutions adsorbed on the microchip and eluted into the FAA spectrometer.

Fig. 5. Reproducibility and time needed for measurements of 30 μL samples of Cr(VI) obtained with FAA spectrometer using micro-injection of the effluents as discrete samples. The effluents were obtained after 0.1 mg/mL solutions of 30 μL volumes are simultaneously loaded to the parallel microcolumns to retain the Cr(VI) and then simultaneously eluted the microcolumns with 30 μL methanol.

269 integrated by the same software, and this integrated area is proportional 270 to the sample concentration loaded onto the microcolumns (Fig. 4d.). 271 The calibration plot of the $Cr(VI)$ standard solutions adsorbed on the mi-272 crochip showed good linearity ($R^2 = 0.9902$). Actually, the determina-273 tion of high concentration ($>$ 20 μg/mL) Cr(VI) is possible by this 274 colorimetric procedure (taking photo and making densitogram) with-275 out using FAAS. For the detection of samples containing less than 276 20 μg/mL concentration (10 μL) Cr(VI), more sensitive atomic spectro-277 metric detection is necessary.

 The adsorbed Cr(VI) was eluted with methanol, and the 30 μL efflu- ents were collected into plastic vessels inserted into the ends of the microcolumns ([Fig. 1](#page-2-0)d). The effluents were analyzed by FAA spectrom- eter using micro-injection of the effluents as discrete samples. The obtained atomic absorption signals (Fig. 4b) are in a good agreement with the photos and densitograms of the microcolumns.

 Making a reproducibility study, 12 effluents were obtained when 285 0.1 mg/mL sample solutions of 30μ L volumes were parallelly loaded 286 to the microcolumns and then parallelly eluted the Cr(VI) into the efflu- ent containers. The 30 μL aliquots of effluents as discrete samples are micro-injected into the FAA spectrometer. From Fig. 5, it can be conclud- ed that 6 measurements could be carried out within 30 s. The RSD% values of the measurements of the 12 effluents were 3.7 and 5.8 for peak heights and peak areas, respectively. These obtained RSD% values were the summed contributions of the precision of the injections of the sample volumes into the microchip, the reproducibility of the 293 adsorption process on the parallel microcolumns and the elution of 294 the adsorbed components, and the precision of the FAAS detection of 295 the discrete samples. 296

In order to obtain a maximum enrichment, we should know the 297 volume by which the adsorbed components can be completely eluted. 298 Increasing the volume of the methanol to elute the previously adsorbed 299 Cr(VI), it was found that 10 μL eluent already washed more than 95% 300 part of the adsorbed components into the effluent container. The effi- 301 ciency of the elution of the adsorbed Cr(VI) was plotted against the 302 volume of the methanol used for the elution (Fig. 6). Although the 303 15 μL would be a proper elution volume in our chromatographic system 304 to obtain the maximum enrichment, the 30 μL volume of the effluent is 305 required for the more sensitive and precise FAAS detection. 306

3.3. Analytical performance 307

One of the main advantages of microfluidics is that a large number of 308 analytical systems (in our work chromatographic separation units) can 309 be arranged on a single microchip; thus, several chromatographic sepa- 310 rations, preconcentrations and elutions can be carried out at the same 311 time. Thus, although the chromatographic separation/enrichment pro- 312 cedures require quite a long time, the separation/preconcentration 313 and FAAS determination of 12 samples needed altogether less than 5 314 min due to the multiplex feature of the proposed system. 315

The overall capacity of the microcolumn (C18, 5 μ m beads, 20 mm \times 316 1 mm \times 0.1 mm) was calculated to be 0.45 μg/mm packing for the 317 Cr(VI). Although the demonstrated microchip included only 20 mm 318 length of packings, the lengths can be largely (e.g. $10 \times$) increased if 319 serpentine and curved channels are used for the packing; thus, the 320 capacity of the microcolumn will be increased as well. Theoretically, 321 the capacity of the column could be increased by thicker packings; how- 322 ever, the thickness of the channel created in the PDMS microchip using 323 soft lithography [24] was not allowed to exceed a maximum of around 324 **0.1 mm.** 325

The adsorption of ion-pair formed Cr(VI) on the C18 column is not 326 strong enough to achieve a high preconcentration factor. A maximum 327 80 μL volume of Cr(VI) could be adsorbed on the 20 mm length of the 328 column, but pumping larger volumes of aqueous solutions will result 329 in the slow immobilization of the adsorbed Cr(VI). The highest 330 preconcentration ($8\times$) was obtained when 80 μL sample volume was 331 loaded onto the microcolumn, and the adsorbed Cr(VI) was eluted 332 into a 10 μL volume. Loading 80 μL samples onto the microchip and 333

Fig. 6. Efficiency study of eluting Cr(VI) previously adsorbed on C18 microcolumn in microchip. Picture about the microcolumn before (a,) and after (b,) Cr(VI) is loaded onto the packing and after the column is eluted with (c,) 2 μL, (d,) 5 μL and (e,) 7 μL methanol. The efficiency of elution of adsorbed Cr(VI) was plotted against the volume of the methanol used for elution (f,).

334 nebulizing the methanolic effluent of 30 μL into the FAA spectrometer, 335 0.0031 μg/mL LOD was obtained $(2.1 \times$ better than obtained with conventional, continuous sample introduction). Based on a few pre- experiments with dyes (e.g. brilliant blue FCF, safranin-O), which 338 adsorb much stronger onto the C18 column, more than $100 \times$ preconcentration factors were obtained by loading only 1–2 mL of samples. These pre-experiments show that a chromatographic system with higher enrichment power should be found in future applications.

343 4. Conclusions and outlook

 In this work, we demonstrated for the first time the interface microfluidic chip-based chromatography with flame atomic spectrome- try. The developed low-cost microchip includes 12 microcolumns of 347 conventional C18 (5 µm) chromatographic particles, making the parallel chromatographic separation/preconcentration and the direct introduc- tion of the effluent into the spectrometer possible. In order to test the hyphenated microchip–FAAS system, the Cr(VI) was selected to be separated/preconcentrated. Although the LOD of the chromium deter- mination in this system was only slightly better than in the convention- al FAAS detection, choosing a chromatographic system in which the analyte is more strongly retained, much higher improvement in LOD could be achieved.

 In general, the on-line hyphenations of the chromatography and the atomic spectrometric detection are more preferred than the off-line combinations; however, the proposed simultaneous preconcentrations of several samples on the microchip and the micro-injection of the efflu- ents as discrete samples are optimal and can be considered "more″ than off-line. The preconcentration of sample solutions requires a relatively long time (1–100 min); however, in the microchip, a large number (e.g. 12) of samples can be preconcentrated at the same time. For the preconcentrations on the microchip, only a peristaltic pump (or a syringe in the field) is needed, and the simultaneous elutions to get effluents for the direct micro-injection should be accomplished right before the FAAS analysis. The proposed method of preconcentration on the microchip and the introduction of the effluent from the chip directly to the nebulizer capillary of the atomic spectrometer combine the advantageous features of the off-line and the on-line hyphenations.

 In this work, the microchip was intended to hyphenate with the most often used atomic spectrometer (FAAS), but the use of graphite furnace AAS seems to be a more advantageous choice, since it only needs a sample of around 10–15 μL, just the volume of the effluent collected at the ends of the microcolumns. On the other hand, there are several FAAS works where only a few-microliter-volume sample was needed for sensitive determination [30,31]. Since C18 reversed- phase silica particles are widely used as the stationary phase in HPLC or 379 solid-phase extraction (SPE), the described chip-based chromatographic system has great potential in many applications (e.g. preconcentration, purification, separation).

 Whitesides et al. [32,33] introduced microfluidic paper-based analytical devices, a new class of point-of-care diagnostic devices that are cheap, easy to use and specifically designed for use in developing countries. Carrying out a colorimetric assay on these microfluidic de- vices, photographing the results with a cellular phone equipped with a camera, and transmitting the image to an expert (clinical, environmen- tal laboratory), obvious advantages of telemedicine can be utilized [\[32\].](#page-6-0) We believe that the hereby proposed chromatography-based microchip with colorimetric assay for the detection of toxic Cr(VI) provides the principle of a similar useful tool.

02 5. Uncited reference

393 [\[29\]](#page-6-0)

Acknowledgments 394

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