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Abstract Spectral resolution in proton NMR spectroscopy is reduced by the splitting of resonances into multiplets due to the effect of homonuclear scalar couplings. Although these effects are often hidden in protein NMR spectroscopy by low digital resolution and routine apodization, behind the scenes homonuclear scalar couplings increase spectral overcrowding. The possibilities for biomolecular NMR offered by new pure shift NMR methods are illustrated here. Both resolution and sensitivity are improved, without any increase in experiment time. In these experiments, free induction decays are collected in short bursts of data acquisition, with durations short on the timescale of  $J$ -evolution, interspersed with suitable refocusing elements. The net effect is real-time ( $t_2$ ) broadband homodecoupling, suppressing the multiplet structure caused by proton–proton interactions. The key feature of the refocusing elements is that they discriminate between the resonances of active (observed) and passive (coupling partner) spins. This can be achieved either by using band-selective refocusing or by the BIRD element, in both cases accompanied by a nonselective 180° proton pulse. The latter method selects the active spins based on their one-bond heteronuclear  $J$ -coupling to  $^{15}\text{N}$ , while the former selects a region of the  $^1\text{H}$  spectrum. Several novel pure shift experiments are presented, and the improvements in resolution and sensitivity they provide are evaluated for representative samples: the N-terminal domain of PGK; ubiquitin; and two mutants of the small antifungal protein PAF. These new experiments, delivering improved sensitivity and resolution, have the potential to replace the current standard HSQC experiments.

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Keywords (separated by '-') Pure shift - Real-time - HSQC - Homodecoupling - Protein

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Footnote Information

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Electronic supplementary  
material

Below is the link to the electronic supplementary material.

**MOESM1:** Supplementary material 1 (DOC 5023 kb).

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2 **Real-time pure shift  $^{15}\text{N}$  HSQC of proteins: a real improvement**  
3 **in resolution and sensitivity**

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5 Juan A. Aguilar · István Timári · Matthew J. Cliff · Mathias Nilsson ·  
6 Péter Sándor · Gyula Batta · Jonathan P. Waltho · Katalin E. Kövér ·  
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15 scenes homonuclear scalar couplings increase spectral  
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**Keywords** Pure shift · Real-time · HSQC ·  
Homodecoupling · Protein

43 **Introduction**

44 To understand relationships between biological structure  
 45 and function, we need tools for the study of complex sys-  
 46 tems, such as proteins and oligonucleotides, that have large  
 47 numbers of constitutionally very similar elements. NMR  
 48 methods provide invaluable detail about both structure and  
 49 dynamics at the atomic level (Tollinger et al. 2001), but  
 50 can be limited by the overlap between resonances from  
 51 multiple individual atomic sites. Indeed, increasing  
 52 resolution has been crucial to broadening the scope of  
 53 biomolecular NMR spectroscopy. The use of very strong  
 54 magnetic fields and multidimensional experiments is now  
 55 standard. Recent improvements in non-uniform sampling  
 56 (Mayzel et al. 2014; Mobli and Hoch 2014) can shorten the  
 57 overall durations of multidimensional NMR experiments,  
 58 and can be used to increase resolution in indirect dimen-  
 59 sions. Improvements in the basic resolution of standard  
 60 protein 2D NMR experiments can translate directly into the  
 61 more complex nD experiments that share building blocks,  
 62 so improving the resolution of the basic HSQC experiment  
 63 is a priority. Unfortunately this can generally only be  
 64 achieved by using higher magnetic fields. While adequate  
 65 sensitivity is usually available from cryogenically cooled  
 66 NMR probes at high magnetic fields (Styles and Soffe  
 67 1984; Kovacs et al. 2005) spectral resolution in the direct  
 68 proton dimension remains a fundamental limiting factor in  
 69 current biomolecular NMR applications.

70 A range of novel methods have been developed for  
 71 small molecules in recent years, that reduce the complexity  
 72 of  $^1\text{H}$  NMR spectra by collapsing the multiplet structure of  
 73 each resonance into a singlet (Zangger and Sterk 1997;  
 74 Nilsson and Morris 2007; Aguilar et al. 2010, 2011;  
 75 Sakhaii et al. 2013; Meyer and Zangger 2014a, b; Castañar  
 76 et al. 2013a, b, 2014a, b; Morris et al. 2010; Sakhaii et al.  
 77 2009; Timári et al. 2014; Reinsperger and Luy 2014;  
 78 Adams et al. 2014). These are often termed “pure shift”  
 79 experiments, because they deliver pure chemical shift in-  
 80 formation without the complication of homonuclear cou-  
 81 pling interactions. In the case of small molecules, valuable  
 82 stereochemical information can often be derived from  
 83 analysis of proton multiplets (Karplus 1959, 1960). How-  
 84 ever, such information is not normally required from the  
 85 HSQC spectra of biomolecules [though there are spe-  
 86 cialised methods available for obtaining it (Permi 2003)].  
 87 Rather, the splitting of proton resonances in HSQC in-  
 88 creases spectral complexity and degrades resolution and  
 89 sensitivity, reducing the value of HSQC and its many  
 90 derivatives in structural biology. There is thus a strong  
 91 incentive to design pure shift HSQC analogues that would  
 92 yield fully decoupled correlation maps, for example a  
 93  $^1\text{H}$ - $^{15}\text{N}$  HSQC spectrum without any splitting due to scalar  
 94 coupling, showing only the  $^1\text{H}$  and the  $^{15}\text{N}$  chemical shifts,

in the direct ( $F_2$ ) and the indirect ( $F_1$ ) dimensions  
 respectively.

Heteronuclear  $^1\text{J}$  couplings are typically very large  
 compared to linewidths, so decoupling them requires rapid  
 spin inversion, and most efficient decoupling schemes use  
 continuous radiofrequency irradiation. In contrast, homonu-  
 cleolar couplings are rarely much more than a factor of 10  
 larger than linewidths, so in principle it should be possible  
 to decouple them with relatively sparse periodic manipulations  
 of the spin system. Pure shift methods typically acquire short  
 chunks of data of duration  $\ll 1/J_{\text{HH}}$  (Zangger and Sterk 1997;  
 Nilsson and Morris 2007; Aguilar et al. 2010) since the  
 evolution of the effects of coupling can be neglected on this  
 timescale. Two types of experiment are in common use: in-  
 terferogram-based, in which a composite free induction de-  
 cay is built up from multiple individual chunks of data of  
 duration  $1/\text{sw}_{\text{ps}}$ , each acquired after an evolution period  $t_{\text{ps}}$   
 that is incremented in steps of  $1/\text{sw}_{\text{ps}}$ ; and real-time, in which  
 blocks of data of duration  $1/\text{sw}_{\text{ps}}$  are acquired one after an-  
 other in the direct dimension ( $t_2$ ). The subscript “ps” refers to  
 the pure shift dimension, which is essentially the same as the  
 direct dimension in a real-time experiment, but requires in-  
 creasing the dimensionality when the interferogram-based  
 strategy is employed. The requirement that each chunk cor-  
 responds to a whole number of data points means that  $\text{sw}_{\text{ps}}$   
 must be an integer submultiple of the direct acquisition  
 spectral width (sw). In each case one of a number of different  
 possible pulse sequence elements can be used to refocus the  
 effects of coupling, either in the middle of  $t_{\text{ps}}$  for an inter-  
 ferogram experiment, or in between acquisition of data  
 chunks in a real-time experiment.

The  $J$ -refocusing pulse sequence elements used all dis-  
 tinguish between active spins, for which signals are to be  
 recorded, and passive spins, for which the effects of cou-  
 plings with active spins are to be suppressed. Since only a  
 minority of spins are observed, there is often (although not  
 invariably) a price in sensitivity and/or experiment time to  
 be paid for the decoupling achieved. Increased experiment  
 time is a particular problem in biomolecular research,  
 where multidimensional experiments are the norm, so here  
 real-time methods that acquire a pure shift FID in a single  
 shot (Lupulescu et al. 2012; Meyer and Zangger 2013;  
 Adams 2014; Kakita and Bharatam 2014) are to be pre-  
 ferred. No special data processing is needed for real-time  
 pure shift NMR experiments, and standard hardware may  
 be used provided that it supports windowed acquisition  
 mode.

A variety of different  $J$ -refocusing elements have been  
 published; each has its own advantages and disadvantages.  
 Here, we compare the performance of BIRD (Bilinear  
 Rotation Decoupling) (Garbow et al. 1982; Aguilar et al.  
 2011) and BASHD [Band-Selective-HomoDecoupling  
 (Brüschweiler et al. 1988; Krishnamurthy 1997)] with that



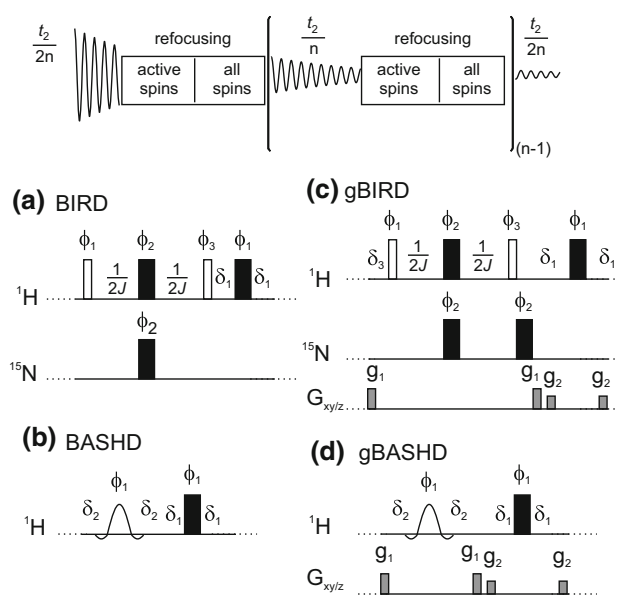
148 of the method currently used for homonuclear decoupling  
 149 during acquisition for proteins, time-shared band-selective  
 150 irradiation (Hammarström and Otting 1994; Kupce and  
 151 Wagner 1995; Kooi et al. 1999; Struppe et al. 2013). The  
 152  $^{15}\text{N}$  HSQC experiment was chosen for the comparison  
 153 because it is among the most important building blocks of  
 154 modern multidimensional experiments, and is widely used  
 155 for screening, e.g. in binding studies and for pH and tem-  
 156 perature dependence; the specific versions used here are the  
 157 multiplicity-edited gHSQC (Boyd et al. 1992) and the  
 158 sensitivity-enhanced gHSQC-SE (Kontaxis et al. 1994;  
 159 Schleucher et al. 1994), but the conclusions should be  
 160 general.

161 We have recently improved the resolution and sensi-  
 162 tivity of the gHSQC experiment for small molecules  
 163 (Paudel et al. 2013) by adding broadband homodecoupling  
 164 using the BIRD (Garbow et al. 1982) element in a real-time  
 165 acquisition scheme (see Fig. 1a). The band-selective analo-  
 166 gue has recently been used to enhance the resolution of  
 167 RDC measurements in partially-oriented proteins (Ying  
 168 et al. 2014). The results of BIRD and BASHD based pure  
 169 shift methods are directly compared here for the first time.  
 170 Water suppression is improved by implementing coherence  
 171 transfer pathway (CTP) selection using pulsed field gradi-  
 172 ents (Fig. 1c, d); the utility of triaxial gradients (Ferrage  
 173 et al. 2003; Sarkar et al. 2008) is also explored.

174 The pure shift  $^{15}\text{N}$  HSQC methods were tested on: (1)  
 175 L80C mutant of the N-terminal domain of phosphoglyc-  
 176 erate kinase in its denaturated state; (2) a globular protein  
 177 (ubiquitin) in its folded state; and (3) two mutants of  
 178 *Penicillium chrysogenum* Antifungal Protein (PAF).

## 179 Materials and methods

180 The pET5 expression vector for wild-type N-PGK com-  
 181 prising residues 1–174 of phosphoglycerate kinase from *G.*  
 182 *stearothermophilus* has been described previously (Parker  
 183 et al. 1996). Mutants were produced by the Quikchange<sup>TM</sup>  
 184 method. BL21(DE3) strains of *E. coli* transformed with the  
 185 appropriate expression vectors were incubated at 37 °C in  
 186 minimal M9 media with [ $^{15}\text{N}$ ]ammonium chloride as the  
 187 sole nitrogen source, and expression was induced by ad-  
 188 dition of 1 mM IPTG once an OD<sub>600</sub> of 0.8 was reached,  
 189 followed by overnight incubation. The expressed protein  
 190 was purified as previously described. The NMR sample of  
 191 (1) contained 20 mM Tris, 20 mM Bistris, 0.5 mM  
 192 ethylenediaminetetraacetic acid, and 3 mM sodium azide,  
 193 at pH 6.0, plus 3.3 M GuHCl, all in 90 % H<sub>2</sub>O/10 % D<sub>2</sub>O.  
 194 The protein concentration was approximately 0.5 mM. The  
 195 uniformly  $^{15}\text{N}$ -labeled ubiquitin sample (1 mM, 90 %  
 196 H<sub>2</sub>O/10 % D<sub>2</sub>O; pH 7.0) was purchased from Cortecnet  
 197 (Giotto Biotech).



**Fig. 1** The generic data acquisition scheme for real-time pure shift NMR methods is shown at the top. The pulse sequence, preceding data acquisition, was either a standard multiplicity edited HSQC with gradient selection (gHSQC) or a gradient selected HSQC with sensitivity enhancement (gHSQC-SE); only the  $J$ -refocusing elements are shown here (a–d) for clarity. The pure shift sequence elements used here were: **a** BIRD; **b** BASHD; **c** BIRD with coherence transfer pathway selection (CTP) gradients denoted by gBIRD; and **d** BASHD with CTP gradient pulses denoted by gBASHD. Delays  $\delta_1$ ,  $\delta_2$  and  $\delta_3$  were usually set to 20  $\mu\text{s}$  (amplifier and receiver blanking), 50  $\mu\text{s}$  (changing power levels on the transmitter) and 208  $\mu\text{s}$  (time correction for the second nitrogen  $180^\circ$  pulse including the corresponding blanking delays), respectively. See Supplementary Material for all details of the pulse programs. Electronic copies of pulse sequences, parameters, and experimental data are available from <http://nmr.chemistry.manchester.ac.uk>. The CTP gradient pulses were applied simultaneously on the  $x$  and  $y$  channels where triaxial gradients were available. The 16 step phase cycle of gHSQC was extended [ $\Phi_1 = \{x, y\}$ ;  $\Phi_2 = \{y, -x\}$ ;  $\Phi_3 = \{-x, -y\}$ ] to 32 in order to suppress the effects of imperfections of the  $J$ -refocusing elements. Employing the full phase cycling is not mandatory (the minimum recommended is two steps), but improves the results for sensitivity-limited applications. See Supplementary Figure 7 and 8 for details

198 The sensitivity-enhanced HSQC experiments were  
 199 recorded using samples of unlabelled (6.5 mM, PAF<sup>D55N</sup>)  
 200 and  $^{15}\text{N}$ -labelled (1.7 mM, PAF<sup>D19S</sup>) mutants of *Penicil-*  
 201 *lium* antifungal protein (PAF) in 95 % H<sub>2</sub>O/5 % D<sub>2</sub>O using  
 202 20 mM Na<sub>3</sub>PO<sub>4</sub> pH 6.0 buffer, 40 mM NaCl, 0.04 %  
 203 NaN<sub>3</sub>, as 275  $\mu\text{L}$  of solution in Shigemi NMR tubes. The  
 204 molecular mass of (3) was  $\sim 6.2$  kDa and the average  
 205 proton  $T_2$  relaxation was  $\sim 55$  ms at 25 °C (estimated from  
 206 linewidth). The proteins were expressed and purified as  
 207 previously described (Batta et al. 2009; Váradi et al. 2013).

208 The NMR experiments on (1) and (2) were carried out  
 209 using an 11.7 T (500 MHz for  $^1\text{H}$ ) Agilent/Varian VNMRs  
 210 spectrometer equipped with a triple resonance HCN triple-  
 211 axis gradient probe of maximum  $xy$  and  $z$  gradients 37.2

212 and  $68.6 \text{ G cm}^{-1}$ , respectively. 960 or 1024 complex  
 213 points were acquired (and zero-filled up to 16,384 complex  
 214 points) at a spectral width of 5 kHz, and 32 scans were  
 215 accumulated in order to achieve the very good signal-to-  
 216 noise ratio needed to allow detailed comparison between  
 217 different methods. Data acquisition in the pure shift ex-  
 218 periments typically consisted of 4–8 chunks. The spectral  
 219 width in the indirect dimension ( $^{15}\text{N}$ ) was 1500 Hz, and  
 220 128 increments (zero-filled up to 1024 complex points)  
 221 were acquired with a 5 s relaxation delay for the L80C  
 222 mutant of the N-terminal domain of phosphoglycerate (**1**).  
 223 In the case of ubiquitin (**2**) the spectral width in the indirect  
 224 dimension ( $^{15}\text{N}$ ) was 2000 Hz and 64 increments (zero-  
 225 filled up to 256 complex points) were acquired with a 3 s  
 226 relaxation delay. The mother experiments, needed for  
 227 comparison, were run with identical experimental pa-  
 228 rameters; the small difference (50–80 ms per transient for  
 229 BIRD, significantly less for BASHD) in acquisition time  
 230 due to the pure shift sequence elements was compensated  
 231 for by adjusting the relaxation delay to give the same  
 232 overall experiment duration. Traditional time-shared ho-  
 233 modecoupling was achieved by using 87 % of the dwell  
 234 time for sampling the free induction decay and 10 % for  
 235 radiofrequency irradiation and 3 % for amplifier blanking  
 236 and T/R switch delays. CTP selection gradient pulses in the  
 237 pure shift elements (gBIRD and gBASHD; see Fig. 1c, d)  
 238 were 0.5 ms long and of 16.6 and  $13.6 \text{ G cm}^{-1}$  amplitude.  
 239 Gradient stabilization delays in the pure shift elements  
 240 were 200  $\mu\text{s}$ . Using too-short gradient stabilization delays  
 241 (strongly dependent on the spectrometer used) can lead to a  
 242 systematic frequency shift (of the order of 2 Hz) in the  
 243 proton dimension, which can be easily corrected by internal  
 244 referencing as normal, or cured by tedious optimization of  
 245 the amplitudes of the CTP gradients using opposite po-  
 246 larities for  $g_1$  and  $g_2$ . Amide band-selective refocusing was  
 247 implemented with reBURP (Geen and Freeman 1991) 180°  
 248 pulses of 2 kHz bandwidth and 2.44 ms duration for (**1**)  
 249 and 2.2 kHz bandwidth and 2.22 ms duration for (**2**) with  
 250 the transmitter offset set to the middle of the amide region.  
 251 (If off-resonance pulses are used it is essential that these be  
 252 phase coherent with the main sequence rather than simply  
 253 being implemented with direct frequency jumps of the  
 254 transmitter channel). In case of the BIRD element,  
 255 Broadband Inversion Pulses (BIP) (Smith et al. 2001) were  
 256 implemented to minimize off-resonance effects, but this  
 257 turned out to be negligible for proteins having reasonably  
 258 small  $^{15}\text{N}$  spectral widths (see Supporting Fig. 4 for a  
 259 comparison). Off-resonance effects are more important for  
 260 small molecules, where efficient inversion is difficult to  
 261 achieve by using rectangular pulses. Time-shared ho-  
 262 modecoupling was achieved by using the standard imple-  
 263 mentation of VnmrJ 4.0 software. Parameters for sample  
 264 (**1**) and (**2**) were the following: constant-adiabaticity

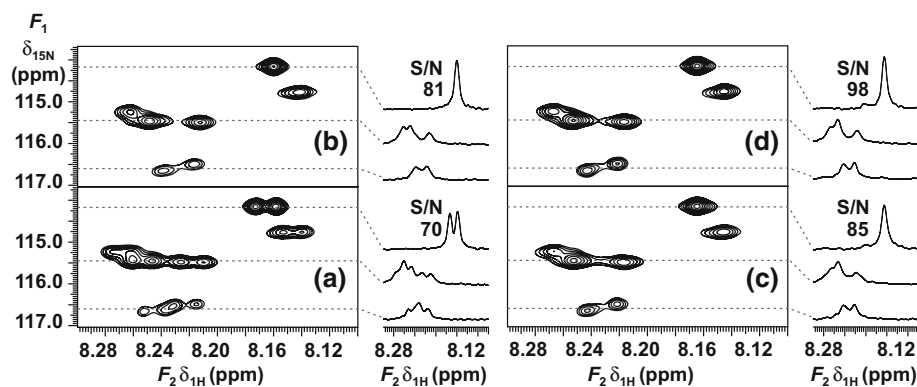
CAWURST pulses with duration of 20 ms; decoupling  
 bandwidth 1500 Hz; adiabaticity 1.2; duty cycle 13 %  
 (87 % sampling, 10 % decoupling and 3 % switching  
 time);  $t_5$  super-cycle (Tycko et al. 1985) phases: 0°, 150°,  
 60°, 150°, 0°. The shaped pulse was created with these  
 parameters, but the pulse shaping program did not take into  
 account the duty cycle. Therefore the power level of the  
 homodecoupling was increased up to, where sufficient  
 decoupling was achieved. Resonance offset for the de-  
 coupling shape was also experimentally fine adjusted:  
 4.5 ppm for (**1**) and 4.0 ppm for (**2**). Experiments were  
 acquired at regulating temperature to +25 °C and the av-  
 erage proton  $T_2$  relaxation of the samples (**1**) and (**2**) was  
 ~60 and ~35 ms (estimated from linewidth).

The pure shift FIDs were automatically concatenated by  
 the spectrometer hardware and all spectra (**1**) and (**2**) were  
 processed identically for the comparison of different  
 methods. Weighting functions were not applied in the di-  
 rect dimension in order to best view the homonuclear  
 couplings. The  $\exp(-t/gf1)/2$  function was used in the  
 indirect dimension, where  $t$  is the time and gf1 was set to  
 0.085 and 0.032 s for sample (**1**) and (**2**) respectively.  
 VnmrJ 4.0 software was used for data acquisition, pro-  
 cessing and plotting. Water presaturation was not used in  
 any of the experiments, and solvent subtraction was not  
 used during data processing.

The NMR experiments on unlabelled and  $^{15}\text{N}$ -labelled  
 mutants of PAF (**3**) were performed at 25 °C on a Bruker  
 Avance II 500 spectrometer equipped with a TXI z-gradi-  
 ent probe (maximum gradient was  $50.1 \text{ G cm}^{-1}$ ), and the  
 resulting data were processed with TopSpin 2.1 or 3.0. The  
 spectra in Fig. 6 were recorded with the following pa-  
 rameters: the spectral widths in  $^1\text{H}$  ( $^{15}\text{N}$ ) dimension were  
 4.788 (21.0) ppm, number of data points in  $^1\text{H}$  dimension  
 was 1024, number of  $t_1$  increments was 128, number of  
 scans was 128, relaxation delay was 1.8 s. Prior to 2D  
 Fourier transformation, the data were apodized by multi-  
 plying with 90° shifted sine-squared function along both  
 dimension and zero-filled up to  $2048 \times 512$  complex  
 points in  $F_2 \times F_1$ . Data acquisition in the pure shift  
 $^1\text{H}$ - $^{15}\text{N}$  HSQC-SE experiment was divided into 8 chunks,  
 and the length of each chunk was 26.7 ms.

## Results and discussion

Partial  $^{15}\text{N}$  HSQC spectra of (**1**) recorded with different  
 acquisition schemes, including gBIRD, gBASHD and  
 conventional time-shared homonuclear decoupling, are  
 compared in Fig. 2. There are two well resolved and five  
 partially overlapping doublets in this region of the HSQC  
 spectrum. In the real-time pure shift spectra, all doublets  
 have collapsed to singlets. Selected traces are shown next



**Fig. 2** Partial  $^1\text{H}$ - $^{15}\text{N}$ -HSQC spectra of the L80C mutant of the N-terminal domain of phosphoglycerate kinase (1) in 3.6 M guanidine hydrochloride in 90 %  $\text{H}_2\text{O}/10$  %  $\text{D}_2\text{O}$ , acquired using **a** HSQC, **b** HSQC with CAWURST time-shared homonuclear decoupling during acquisition, **c** pure shift gBIRD-HSQC, and **d** pure shift

gBASHD-HSQC. Selected traces are shown at  $\delta_{15\text{N}}$ : 114.15, 115.34 and 116.55 ppm, respectively. Signal-to-noise ratio is given for the top traces ( $\delta_{15\text{N}} = 114.15$  ppm), which are not distorted by overlapping of resonances. The other two traces are shown to compare the resolution enhancement that was achieved by homodecoupling in **b-d**

315 to each contour plot to illustrate performance. The less  
316 shielded resonances, around 8.24 ppm, show severe spec-  
317 tral overlap in the standard HSQC spectrum. There are two  
318 and three overlapping doublets at  $\delta_{15\text{N}} = 116.55$  ppm  
319 (bottom trace) and  $\delta_{15\text{N}} = 115.34$  ppm (middle trace) re-  
320 spectively. Separate integration of these cross-peaks is  
321 clearly impossible in the standard HSQC spectrum because  
322 of the overlapping multiplet structures. Neither automated  
323 nor manual peak-picking can determine all chemical shifts  
324 accurately in this region, particularly when short acqui-  
325 sition times (<100 ms) and line-broadening weighting  
326 functions mask the fine structure of the amide resonances.  
327 Pure shift NMR is a powerful tool in this example because  
328 each resonance appears as a single peak, making peak  
329 picking relatively trivial. All the five chemical shifts are  
330 resolved for peak-picking in the homodecoupled spectra,  
331 see bottom and middle cross-sections of Fig. 2b-d. There is  
332 relatively little difference between the pure shift spectra at  
333 first glance, but systematic comparison revealed that the  
334 resonances are slightly broader in the BIRD spectrum. This  
335 can be rationalized by the effect of  $T_2$  relaxation during the  
336 longer  $J$ -refocusing elements in BIRD. The implementation  
337 of the traditional time-shared homodecoupling also im-  
338 proves resolution in this example, but it has some major  
339 drawbacks, discussed below, that hamper its routine  
340 application.

341 Besides enhancing the resolution, the real-time pure  
342 shift method also improves the sensitivity of the HSQC  
343 experiment, slightly but usefully. Signal-to-noise ratios are  
344 given for the most shielded resonance at  $\delta_{15\text{N}} = 114.15$   
345 ppm in each experiment in Fig. 2. The highest signal-to-  
346 noise ratio was achieved by gBASHD and corresponded to  
347 c.a. 40 % enhancement relative to the standard HSQC  
348 spectrum (Fig. 2a). However, this sensitivity enhancement  
349 will vary from resonance to resonance, for the following

350 reasons. (1) The natural linewidths are not small compared  
351 to homonuclear  $J$ -couplings in proteins, so the theoretical  
352 maximum sensitivity enhancement, that is a factor of  
353 +100 % for doublets and triplets, is rarely achievable. The  
354 enhancement factor is larger for resonances with larger  
355 homonuclear couplings or longer  $T_2$  relaxation, but smaller  
356 for resonances with unresolved couplings. (2) There is a  
357 sensitivity penalty for real-time acquisition that is depen-  
358 dent on the duration of the  $J$ -refocusing sequence element.  
359 This is the main reason why the sensitivity of the band-  
360 selective method is slightly higher than that of BIRD for  
361 proteins. (3) Sensitivity is clearly affected by the efficiency  
362 of homodecoupling, which varies between methods. BASHD  
363 and time-shared methods are less effective at the edges of  
364 the selected frequency band, while the BIRD  
365 element is longer which leads to more relaxation loss  
366 between the data acquisition periods.

367 In summary, both sensitivity and resolution will gener-  
368 ally improve for resonances showing multiplet structures in  
369 the HSQC spectrum. Radiofrequency pulse imperfections  
370 and  $T_2$  relaxation during the  $J$ -refocusing double spin echo  
371 elements of the acquisition blocks cause some extra loss of  
372 magnetization in the real-time pure shift experiments as  
373 compared to the mother experiment (Paudel et al. 2013).  
374 This leads to resonances in the pure shift spectrum that,  
375 while narrower than the multiplet they replace, are slightly  
376 broader than an individual multiplet component. However,  
377 significant loss of sensitivity is only expected when the  
378 natural line width becomes larger than the scalar couplings,  
379 at which point pure shift methods are in any case inap-  
380 propriate. The sensitivity gain from homodecoupling for a  
381 doublet vanishes around  $J T_2 = 0.1$ , where the coupling  
382 becomes unresolved (Kupce et al. 2002). In the ex-  
383 periments described here, real-time pure shift NMR im-  
384 proved the sensitivity usefully (typically by 30 %), on (1).

385 Slightly better results were achieved using BASHD than  
 386 BIRD, because the  $J$ -refocusing block between data  
 387 acquisition blocks is shorter in the former. Notably, the du-  
 388 ration of the BIRD element is  $1/J_{\text{NH}}$  (typically 11.1 ms)  
 389 independently of the field strength, whereas the length of  
 390 the BASHD element spanning the amide proton region of  
 391 proteins (2.4 ms here) scales inversely with field strength.  
 392 Therefore, at higher magnetic fields the advantage of the  
 393 BASHD method increases. Conventional homo-nuclear  
 394 decoupling by time-shared band-selective irradiation  
 395 (Fig. 2b) also results in improved resolution, but has some  
 396 significant disadvantages making this method unable to  
 397 meet with the needs of most biomolecular applications.  
 398 First, the exact positions of the peaks differ from the true  
 399 chemical shifts because of the Bloch–Siegert effect (Bloch  
 400 and Siegert 1940). Second, the water resonance lies within  
 401 the chemical shift region of  $\text{C}_\alpha\text{H}$  so the band-selective ir-  
 402 radiation very significantly reduces the efficiency of water  
 403 suppression. This problem will be discussed in detail later.  
 404 Third, the dwell time between data points is shared be-  
 405 tween acquisition (87 % of the dwell time) and decoupling  
 406 period, reducing the sensitivity advantage of decoupling by  
 407 about 7 % (Kupce et al. 2002). The signal-to-noise ratio  
 408 difference observed here between time-shared ho-  
 409 modecoupling (Fig. 2b) and real time gBASHD (Fig. 2d)  
 410 experiments was significantly larger, apparently because of  
 411 the increased  $t_2$ -noise caused by imperfect water suppres-  
 412 sion in the former case.

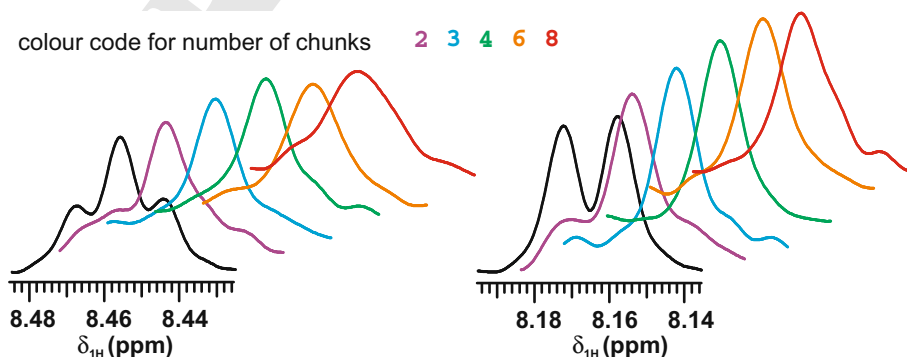
413 All three decoupled spectra (b) to (d) in Fig. 2 show  
 414 better sensitivity than the parent HSQC spectrum (a). The  
 415 selected traces were plotted under identical conditions to  
 416 allow direct comparison of sensitivity and line-width.  
 417 BASHD outperformed BIRD, and both showed slightly  
 418 better sensitivity, and much better resolution, than standard  
 419 HSQC.

420 Although real-time pure shift acquisition adds to the  
 421 complexity of an HSQC pulse sequence, only two

422 additional basic parameters need to be chosen. They are the  
 423 characteristics of the  $J$ -refocusing element (the duration  
 424  $1/J_{\text{NH}}$  of the BIRD element, or the bandwidth and pulse  
 425 shape of the BASHD selective refocusing pulse), and the  
 426 duration  $1/\text{sw}_{\text{ps}}$  of the basic data acquisition chunk. The  
 427 former can easily be automated and does not require input  
 428 from the user. The latter is a compromise between the  
 429 requirements to minimise homonuclear  $J$ -evolution, and to  
 430 minimise signal losses through relaxation during and pulse  
 431 imperfections in the  $J$ -refocusing element. If too small an  
 432  $\text{sw}_{\text{ps}}$  is used (longer chunks),  $J$ -evolution will lead to im-  
 433 perfect decoupling and the appearance of sidebands at  
 434 multiples of  $\text{sw}_{\text{ps}}$ . If  $\text{sw}_{\text{ps}}$  is too large (shorter chunks),  
 435 frequent application of  $J$ -refocusing will lead to excessive  
 436 signal loss and hence line broadening.

437 For the systems studied here, a total acquisition time  
 438 about 200 ms per measurement is needed to make full use  
 439 of the resolution improvement offered by pure shift  
 440 methods. The choice of  $\text{sw}_{\text{ps}}$  (and hence of the number of  
 441 chunks) determines the balance between spectral artefacts  
 442 and line broadening, as illustrated in Fig. 3. Two sets of  
 443 traces, at different nitrogen chemical shifts, through the  $F_2$   
 444 dimension of different HSQC spectra are shown. The traces  
 445 plotted in black are from a conventional HSQC spectrum,  
 446 with no homodecoupling; the remainder are from BIRD-  
 447 decoupled spectra with increasing values of  $\text{sw}_{\text{ps}}$  and hence  
 448 number of chunks needed to form the 200 ms long free  
 449 induction decay. The purple traces, acquired with data  
 450 acquisition chunks of 102.4 ms each ( $\text{sw}_{\text{ps}} = 9.7$  Hz),  
 451 clearly show the expected sidebands at  $\pm\text{sw}_{\text{ps}}$ , but by the  
 452 green pair, corresponding to 4 chunks of 51.2 ms  
 453 ( $\text{sw}_{\text{ps}} = 19.5$  Hz) the sidebands are negligible.

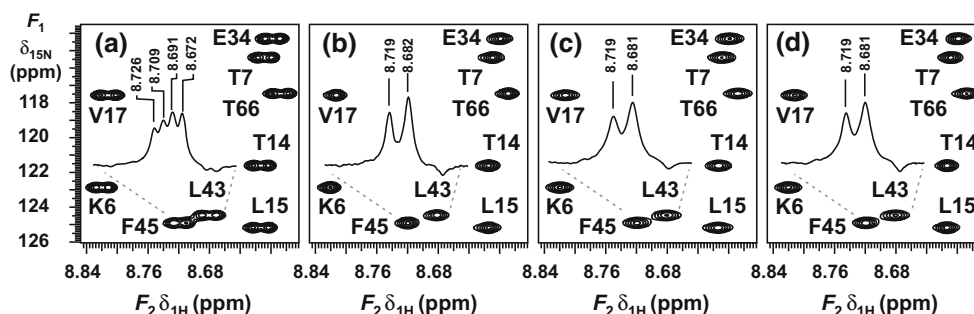
454 Increasing the number of chunks (and  $\text{sw}_{\text{ps}}$ ) further  
 455 simply results in a slight line broadening, as signal losses  
 456 through relaxation and pulse imperfection increase. As  
 457 noted earlier, a very small systematic shift in proton fre-  
 458 quency, typically  $<2$  Hz, can occur, which arises from



**Fig. 3** Selected  $F_2$  traces at  $\delta_{15\text{N}} = 112.00$  ppm (left) and  $\delta_{15\text{N}} = 114.15$  ppm (right) from the conventional HSQC spectrum (black) and from BIRD pure shift HSQC spectra (colour coded) of

(1), showing the effect of increasing the number of data acquisition chunks: 2 purple; 3 blue; 4 green; 6 orange and 8 red (i.e. increasing  $\text{sw}_2$  from 9.7 to 39.1 Hz) for a total acquisition time of c.a. 200 ms



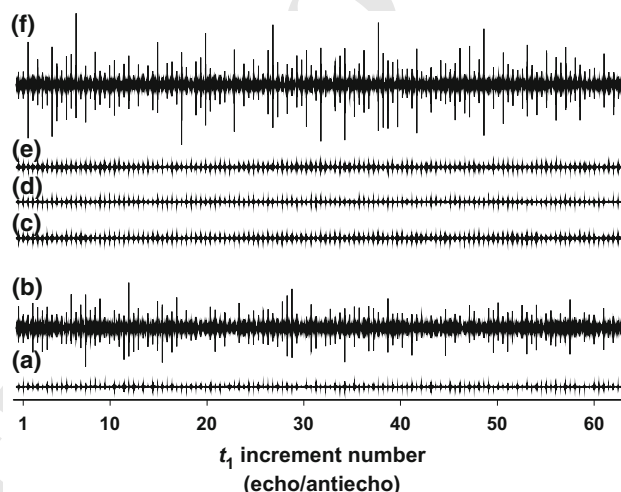


**Fig. 4** Partial  $^1\text{H}$ - $^{15}\text{N}$ -HSQC spectra of  $^{15}\text{N}$ -ubiquitin in 90 %  $\text{H}_2\text{O}/10$  %  $\text{D}_2\text{O}$  (**2**) acquired by using **a** HSQC, **b** HSQC with CAWURST homonuclear decoupling during acquisition, **c** pure shift gBIRD-HSQC and **d** pure shift gBASHD-HSQC

459 finite gradient field recovery time; this effect was corrected  
460 by appropriate referencing. Alternatively, it is possible to  
461 cure the problem at source by alternating signs and mag-  
462 nitudes of successive gradient pulse pairs to cancel the  
463 average field error.

464 The real-time pure shift experiments were also applied  
465 to  $^{15}\text{N}$ -ubiquitin (**2**), to facilitate comparison with standard  
466 methods, this time with 6 data chunks acquired in 200 ms  
467 ( $\text{sw}_{\text{ps}} = 30$  Hz). The resolution enhancement achieved by  
468 different homodecoupling schemes is shown in Fig. 4.  
469 Both the time-shared homodecoupling and the pure shift  
470 methods reduce the spectral complexity by collapsing the  
471 multiplets to singlets. Here the narrowest lines were ob-  
472 served when using time-shared decoupling, but the water  
473 signal suppression was about an order of magnitude worse  
474 than for the real-time pure shift approaches, which would  
475 represent a significant obstacle to practical application.

476 In general, water suppression is particularly challenging  
477 for experiments that use homonuclear decoupling. Prob-  
478 lems arise for real-time pure shift experiments because the  
479 double spin echo element inverts the magnetization of  
480 passive spins, which unfortunately includes that of water  
481 magnetization, from chunk to chunk. Because of radiation  
482 damping, water  $z$ -magnetization is partially transferred to  
483 the  $xy$  plane by the pure shift elements even with perfect  
484 radiofrequency pulses. A seemingly trivial solution would  
485 be to flip back water magnetization selectively during the  
486 double spin echo, but this would affect those  $\text{C}_\alpha\text{H}$  reso-  
487 nances close to or under the water resonance, leading to  
488 recoupling effects for the NH residues coupled to them. A  
489 better solution is to apply CTP selection gradient pulse  
490 pairs around the  $180^\circ$  rotations and extend the phase cycle  
491 by using 2 steps of EXORCYCLE on the pure shift ele-  
492 ments. The use of CTP selection gradient pulses reduces  
493 the residual water signal by more than an order of mag-  
494 nitude, to a level comparable to that in a normal HSQC  
495 experiment. The minimum number of transients required is  
496 the same for pure shift and normal HSQC methods, but if  
497 more transients are used to improve sensitivity then



**Fig. 5** Residual water signal intensity in sample (**2**) as a function of  $t_1$  in **a** standard HSQC; **b** BASHD-HSQC (no PFG pulses in the pure shift element); **c** gBASHD-HSQC using only  $z$  gradient pulses and **d** simultaneous  $xy$  gradients to enforce CTP selection in the pure shift elements; **e** gBIRD-HSQC using  $xy$  gradients; **f** HSQC with time-shared CAWURST homonuclear decoupling during acquisition. All spectra were plotted with *identical vertical scale*. Water presaturation was not used

implementation of the extended phase cycle can improve 498  
the results. Neither flip back nor CTP selection is possible 499  
for the time-shared decoupling, leaving water suppression 500  
as a major problem for this technique. 501

502 Interestingly, the quality of pure shift spectra is influ-  
503 enced not only by the strength but also by the direction of  
504 the CTP selection gradient pulses. Figure 5 compares the  
505 water signal intensity in standard HSQC (Fig. 5a) and real  
506 time BASHD experiments without (Fig. 5b) and with  
507 gradient pulses applied along the  $z$  axis (Fig. 5c) or in the  
508 transverse ( $xy$ ) plane (Fig. 5d). Only the gradient pulses  
509 between the chunks were changed; other gradient pulses  
510 remained along the  $z$  axis. The strengths of the transverse  
511 gradient pulses were matched to the  $z$  gradient pulses by  
512 comparing the signal attenuation in DOSY (Nilsson et al.

513 2004) experiments. Transverse gradient pulses dephase the  
 514 water magnetization more dependably, reducing unwanted  
 515 signal in the 2D spectrum. If water suppression is crucial  
 516 for a protein sample (e.g. because of low concentration or  
 517 natural abundance) then triple gradient axis systems can  
 518 give better results. The BIRD element also affects the  
 519 water magnetization, and similar results were observed  
 520 when adding CTP gradient pulses to the BIRD experiment  
 521 (Fig. 5e).

522 As noted earlier, homodecoupling by time-shared irradiation with CAWURST pulses nicely enhances resolution,  
 523 but water suppression is about an order of magnitude worse  
 524 compared to real-time pure shift experiments, because the  
 525 pulses are applied to the  $C_{\alpha}H$  resonances and hence also  
 526 affect water magnetization. The poor water suppression  
 527 and Bloch–Siegert shifts of resonances seen with time-  
 528 shared irradiation have hampered the routine application  
 529 of homodecoupling in protein NMR spectroscopy to date. The  
 530 new real-time pure shift experiments can deliver good  
 531 homodecoupling without such complications.

532 To check the power and robustness of the gradient enhanced, BIRD-based broadband homodecoupling scheme of  
 533 Fig. 1c, sensitivity-enhanced  $^{15}N$  HSQC spectra were  
 534 recorded using the pulse sequence of Fig. S6 on samples of a  
 535 non-labelled (6.5 mM) (Fig. 6) and  $^{15}N$ -labelled (1.7 mM)  
 536 (Fig. S1 in Supplementary Material) mutant of *Penicillium*  
 537 antifungal protein (PAF, 55 amino acid residue) in 95 %  
 538  $H_2O/5\%$   $D_2O$ . The beneficial features of the pure shift  
 539 HSQC sequence are illustrated in Fig. 6, which compares  
 540 the sensitivity-enhanced HSQC spectra and representative  
 541  $F_2$  traces of the non-labelled PAF $^{D55N}$  mutant recorded  
 542 with the standard (black) and homodecoupled sequences (red). As  
 543  
 544

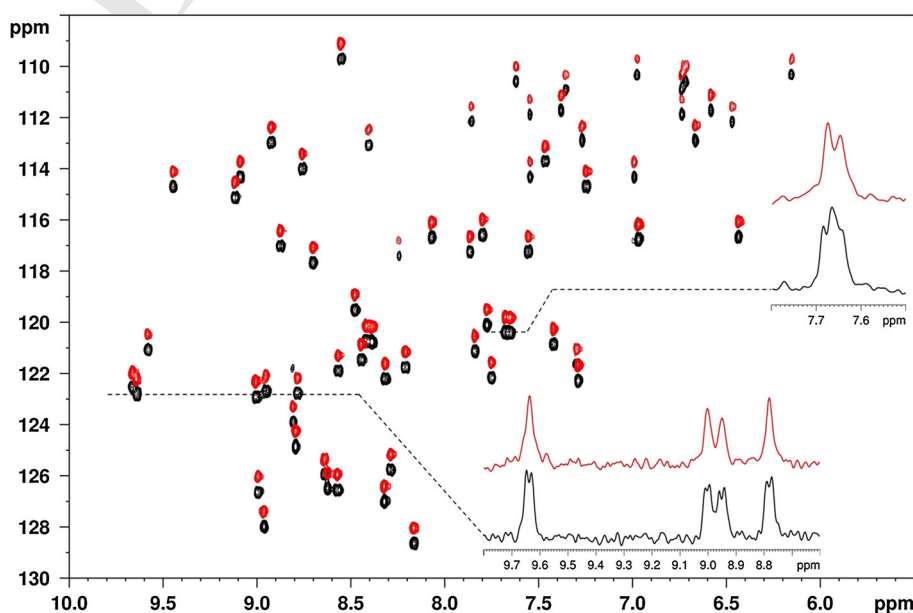
545 expected, decoupling of proton–proton interactions yields a  
 546 reduction in the linewidths observed, resulting in consider-  
 547 ably improved resolution and so allowing unequivocal  
 548 definition of peaks for automated data analysis.

549 The purging and coherence selection gradient pulse  
 550 scheme employed in the sensitivity-enhanced pure shift  
 551 HSQC sequence eliminates the strong water signal very  
 552 efficiently, yielding clean and artefact-free spectra. The  
 553 results shown clearly demonstrate that the pure shift  
 554 methods proposed here are suitable for the study of small  
 555 proteins at low ( $^{15}N$  labelled) and standard concentrations.

## 556 Conclusions

557 Practical homonuclear decoupling has been demonstrated  
 558 for  $^{15}N$  HSQC spectra of proteins without any increase in  
 559 experiment time. Such methods provide an increase in both  
 560 resolution and sensitivity, so long as  $T_2$  is not limiting (in  
 561 practice, for small proteins and for naturally disordered  
 562 regions of larger proteins). Real-time pure shift ex-  
 563 periments suffer from some sensitivity loss due to proton  
 564  $T_2$  relaxation, which also leads to slight broadening of the  
 565 resonances. The collapse of multiplet structures into sin-  
 566 glets compensates for the reduced sensitivity. BASHD  
 567 performs slightly better than BIRD in this respect, because  
 568 it uses a shorter  $J$ -refocusing pulse sequence element. The  
 569 best resolution and sensitivity is however achieved with  
 570 time-shared homodecoupling, provided that the poorer  
 571 water suppression and the Bloch–Siegert effects can be  
 572 tolerated. Both BASHD- and BIRD-based real-time pure  
 573 shift methods deliver significantly better water suppression

**Fig. 6**  $^1H$ - $^{15}N$  HSQC-SE spectra of unlabelled mutant PAF $^{D55N}$  (3) in 95 %  $H_2O/5\%$   $D_2O$  without (black, lower) and with (red, upper) real-time pure shift gBIRD acquisition. The pure shift spectrum is shifted in the nitrogen dimension for easier comparison. The top right inset shows two overlapping peaks



574 than homodecoupling by time-shared irradiation. In practice, the same level of water suppression can be achieved as in standard HSQC experiments if coherence transfer pathway selection with pulsed field gradients is used during data acquisition. The use of triaxial gradients is helpful, but not essential.

580 Pure shift methods are only useful where multiplet splittings are comparable to or greater than natural linewidths. If the natural linewidth is much greater than the homonuclear coupling then the disadvantages outweigh any advantages. In all other systems, real-time pure shift acquisition schemes should be able to replace normal acquisition, offering better resolution and similar or better sensitivity with no penalty in experiment time. The real-time pure shift acquisition schemes presented here should be compatible with any HSQC pulse sequence. Further exploration of their potential to improve standard 3D experiments (e.g. backbone assignment) is ongoing. A particularly important advantage of real-time pure shift methods over normal acquisition in  $^{15}\text{N}$  HSQC is that automatic peak-picking algorithms should no longer require that extra line broadening be used to obscure the fine structure of resonances. In a pure shift spectrum there is only one response from each chemically non-equivalent proton, making it ideal for chemical shift assignment.

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